

Readout Electronics for SiPM Arrays Used for Nuclear Medical Imaging

William W. Moses¹, Martin Janecek¹, Patrick J. McVittie¹,
Jean-Pierre Walder¹, Bob Zheng¹, Henrik von der Lippe¹,
Woon-Seng Choong¹, Qiyu Peng¹, Chinh Vu¹, Mickel McClish²,
Purushottam Dokhale², Christopher J. Stapels²,
James F. Christian², and Kanai S. Shah²

¹*Lawrence Berkeley National Laboratory* and ²*RMD, Inc.*

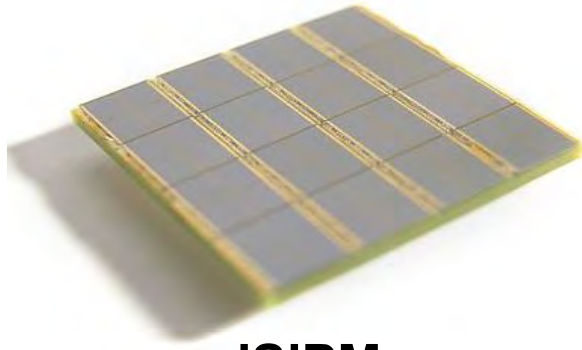
November 3, 2011

-
- **SiPM Readout ASIC**
 - **OpenPET Electronics**

• This work was supported in part by the U.S. DOE (contract No. DE-AC02-05CH11231) and in part by the NIH (NIBIB grant No. R01-EB006085)

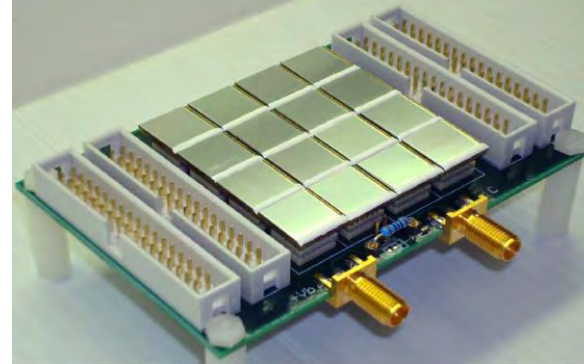
Large Variety of SiPM Arrays Available

Philips



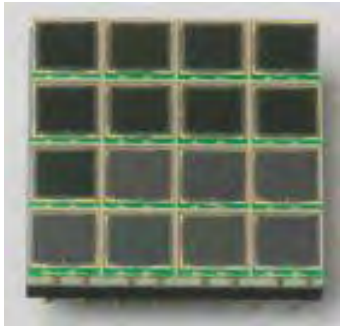
dSiPM

RMD



SSPM

Hamamatsu



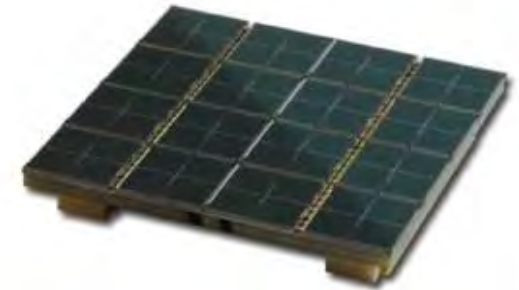
MPPC

SensL



SPM

FBK

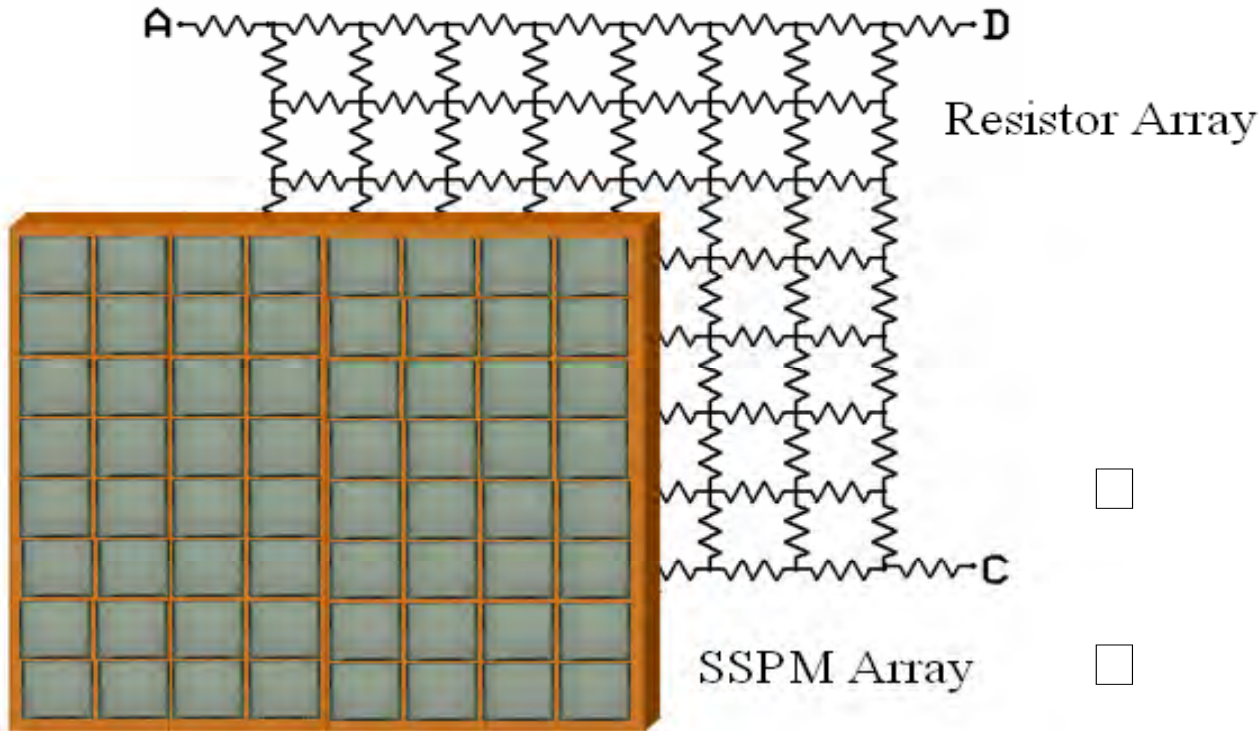


SiPM

- Very Attractive for PET
- Properties Vary (20 pF – 900 pF, \propto Pixel Area)

Channel Count Reduction Needed for PET!

~100,000 detector elements in a PET Camera



$$X = \frac{A + B}{A + B + C + D}$$

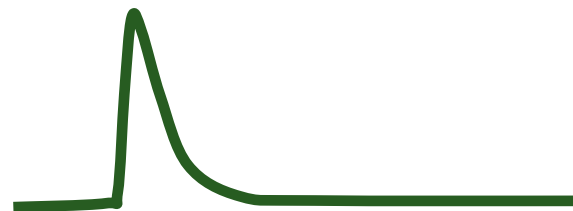
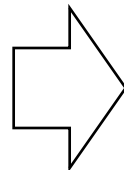
$$Y = \frac{A + D}{A + B + C + D}$$

$$E = A + B + C + D$$

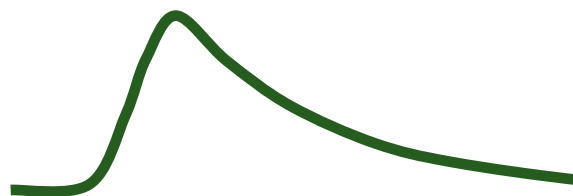
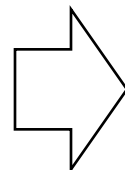
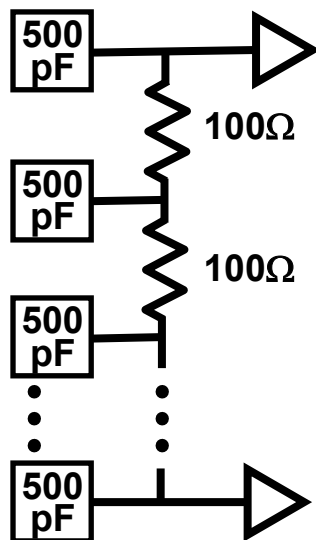
- Current Division → 16-fold Reduction for 8x8 Array
- Standard Technique for PET w/ Multi-Anode PMTs
- Many Commercial PET Cameras Use Similar Readout

Resistor Array Degrades Timing

Single
SiPM Pixel

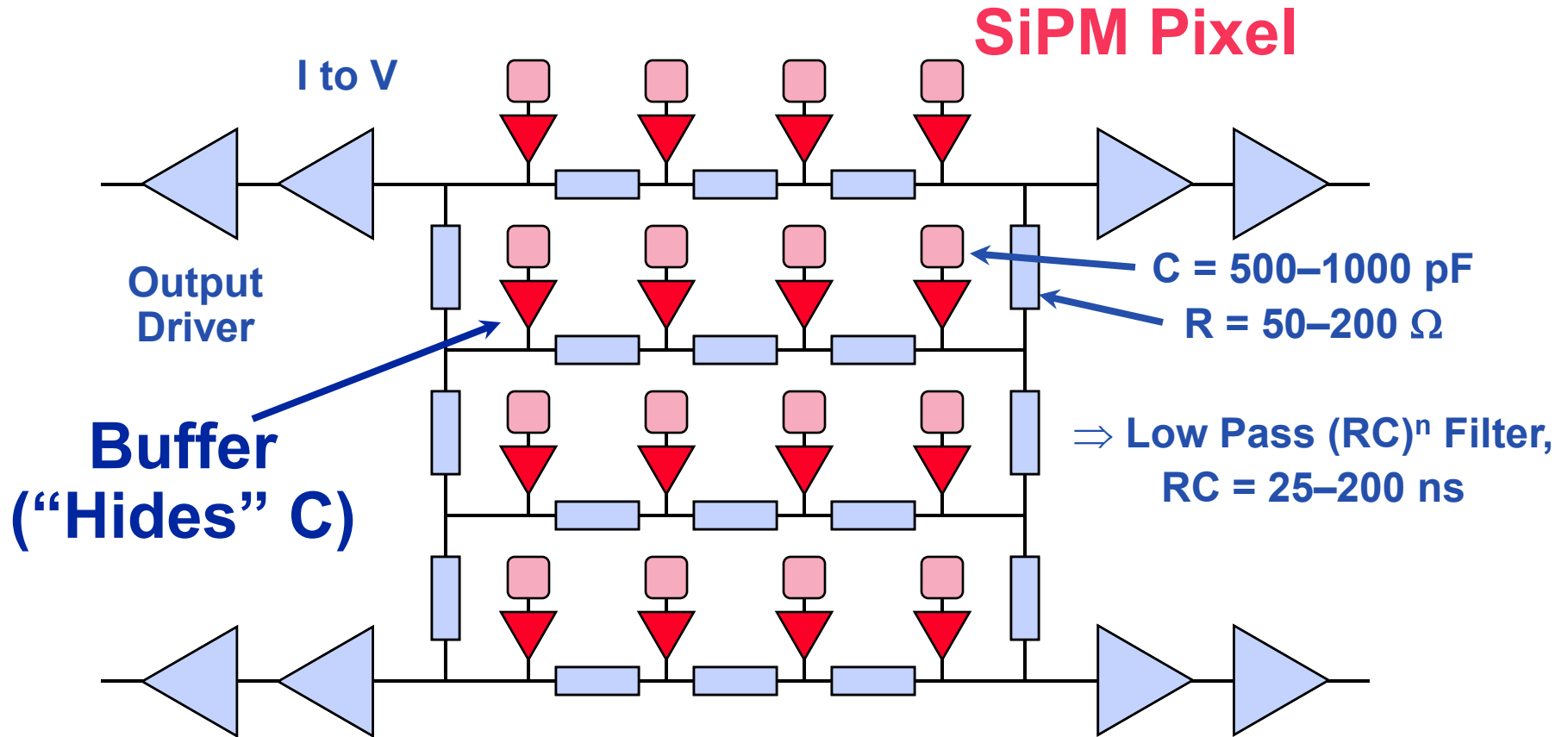


Array of
SiPM Pixels



Multi-Pole RC Filter

ASIC Block Diagram

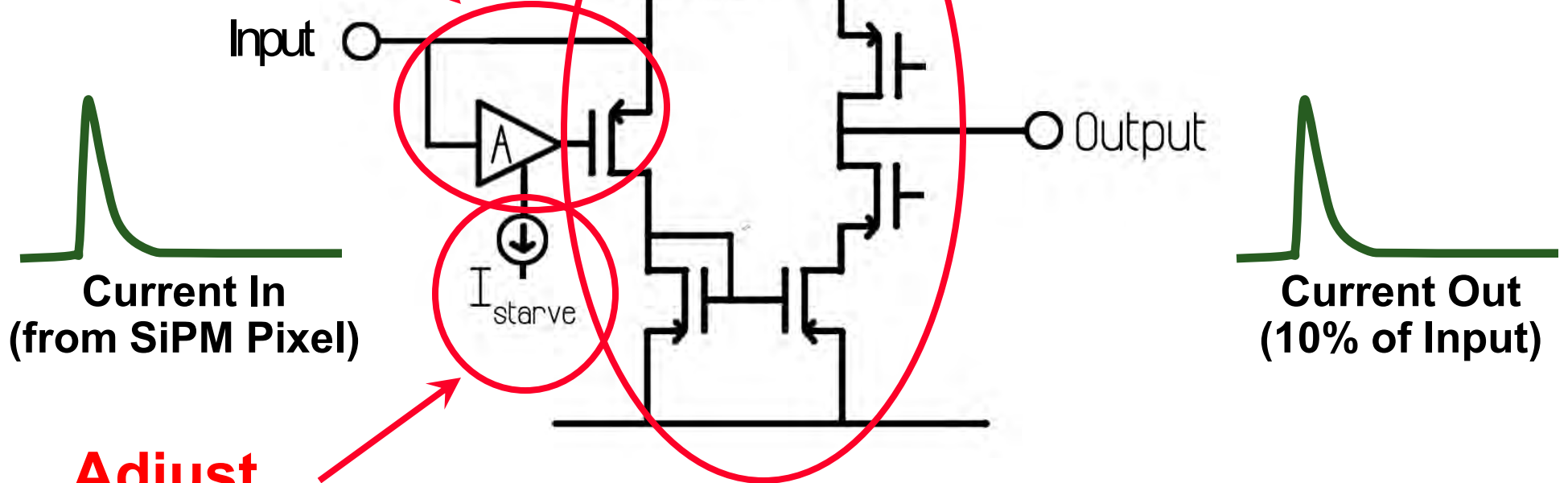


- **Insert Buffer Between SiPM & Resistor Array**
 - **Restores Timing Properties**

Current-Current Converter

**Amplifier
(maintains
V at Input)**

**Current Mirror
(10% of Input)**



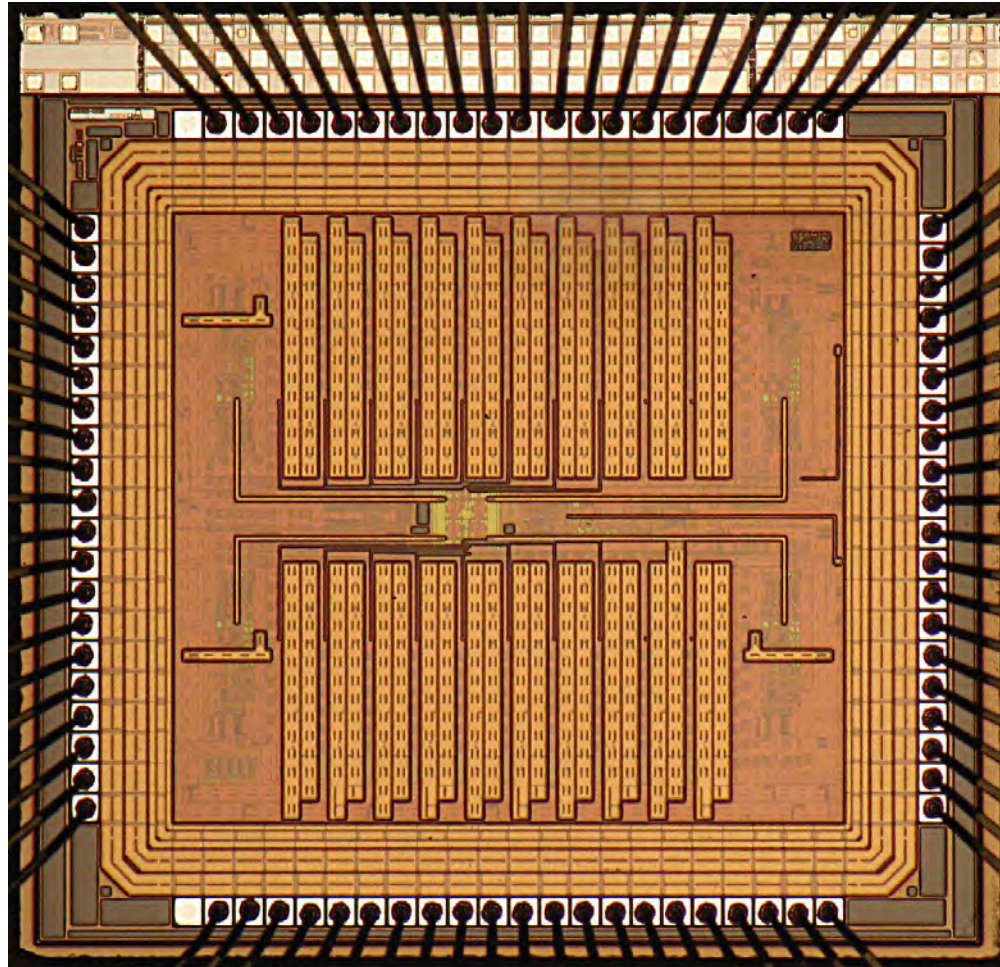
**Current In
(from SiPM Pixel)**

**Current Out
(10% of Input)**

**Adjust
based on
pixel C**

2 ns Rise Time

Photograph of 16-Input Prototype (Photo Required for *All* ASIC Presentations)

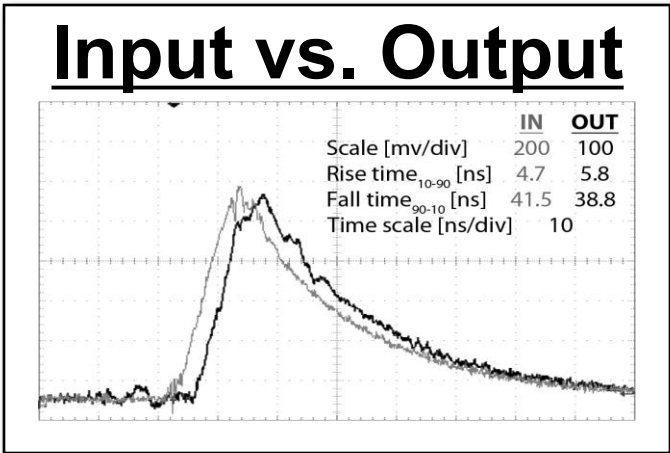


AMS 0.35 μm
TSMC CMOS,
high voltage

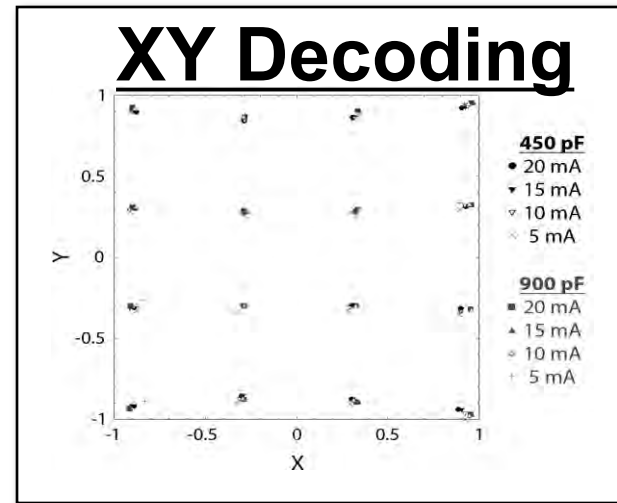
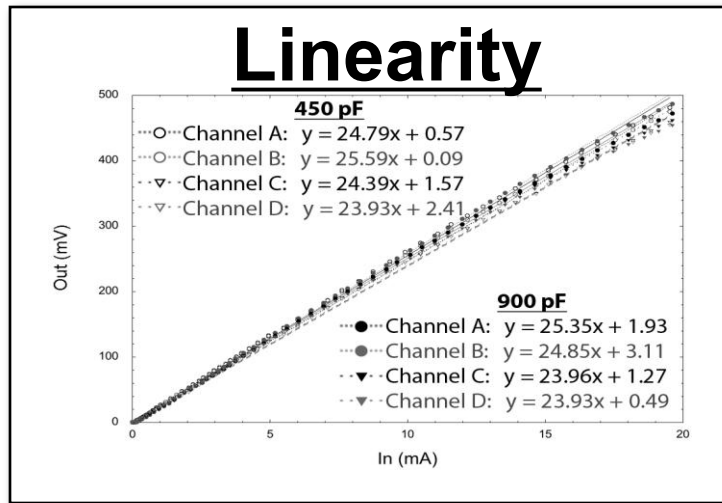
Chip Dimensions:
2.5 mm x 2.5 mm

64-Input Version Just Back from Foundry...

Performance Tests (16-Channel) w/ Pulser

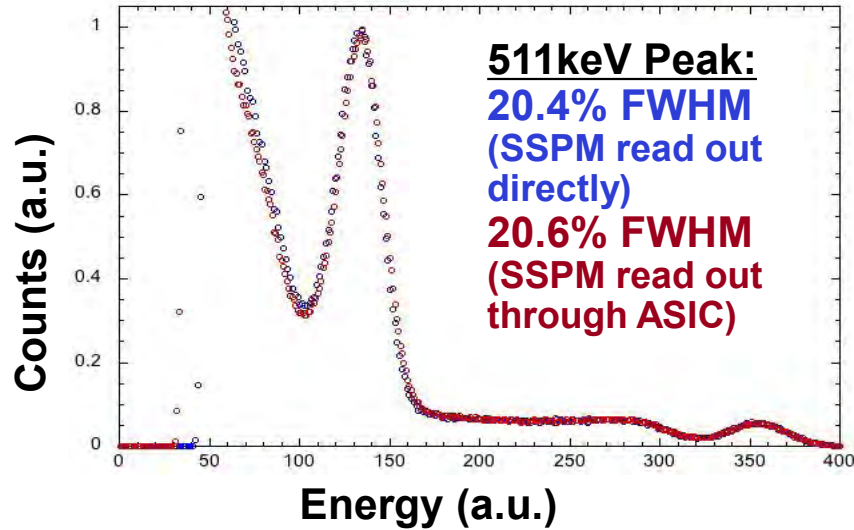


Input Rise Time: 4.7 ns
Output Rise Time: 5.8 ns

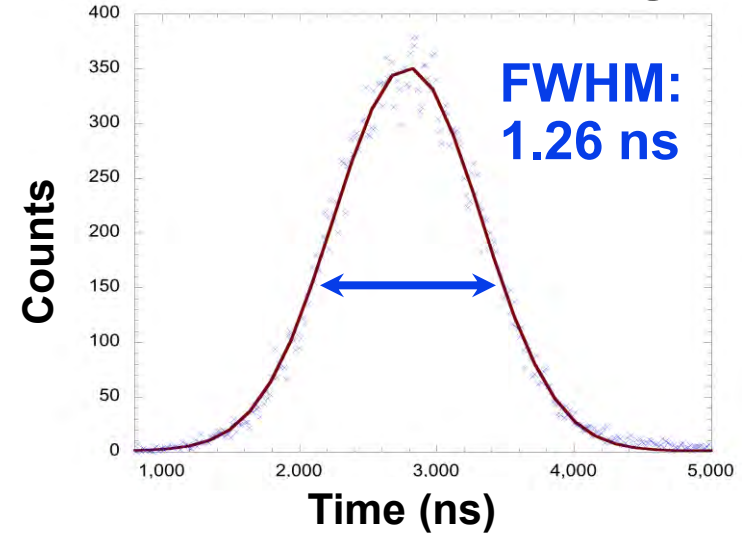


Performance Tests (16 Channel) w/ LSO Array

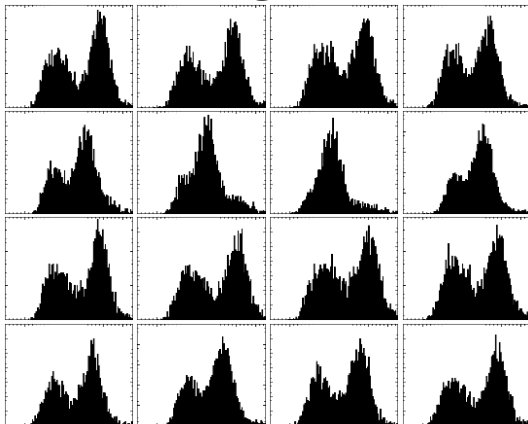
Pulse Height Spectrum



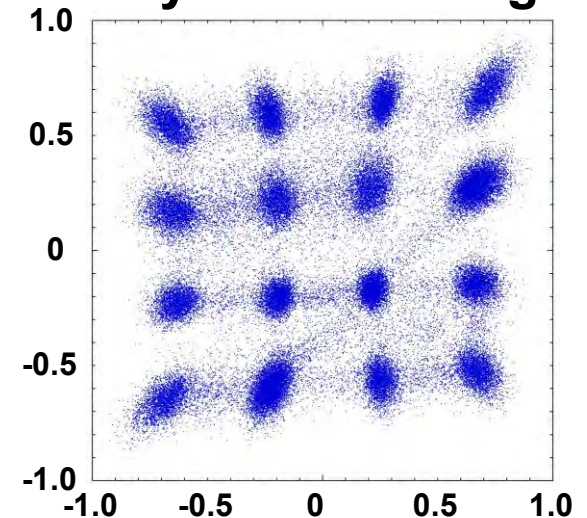
Coincidence Timing



Pulse Height Spectra



Crystal Decoding



It Works!!!

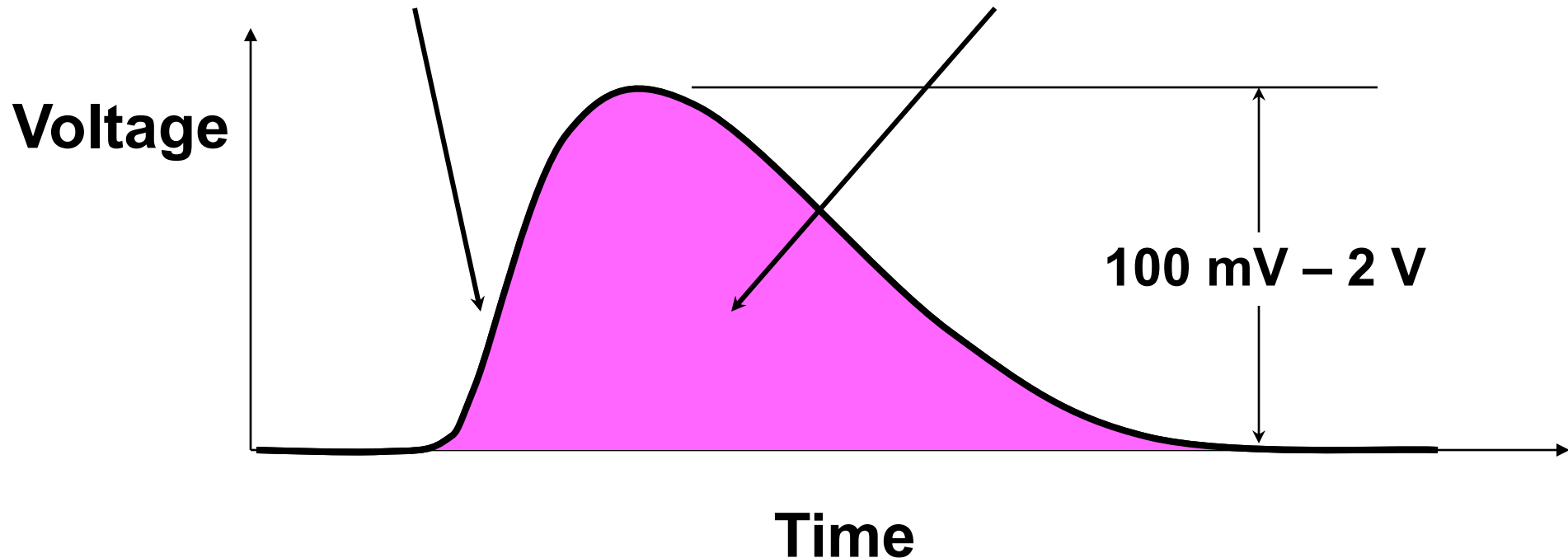
openPET

- Nuclear Medicine Research Community Needs “Industrial-Strength” Electronics
- Needs Can Be Met By Single, *Flexible* Design!

All Detector Outputs Look the Same

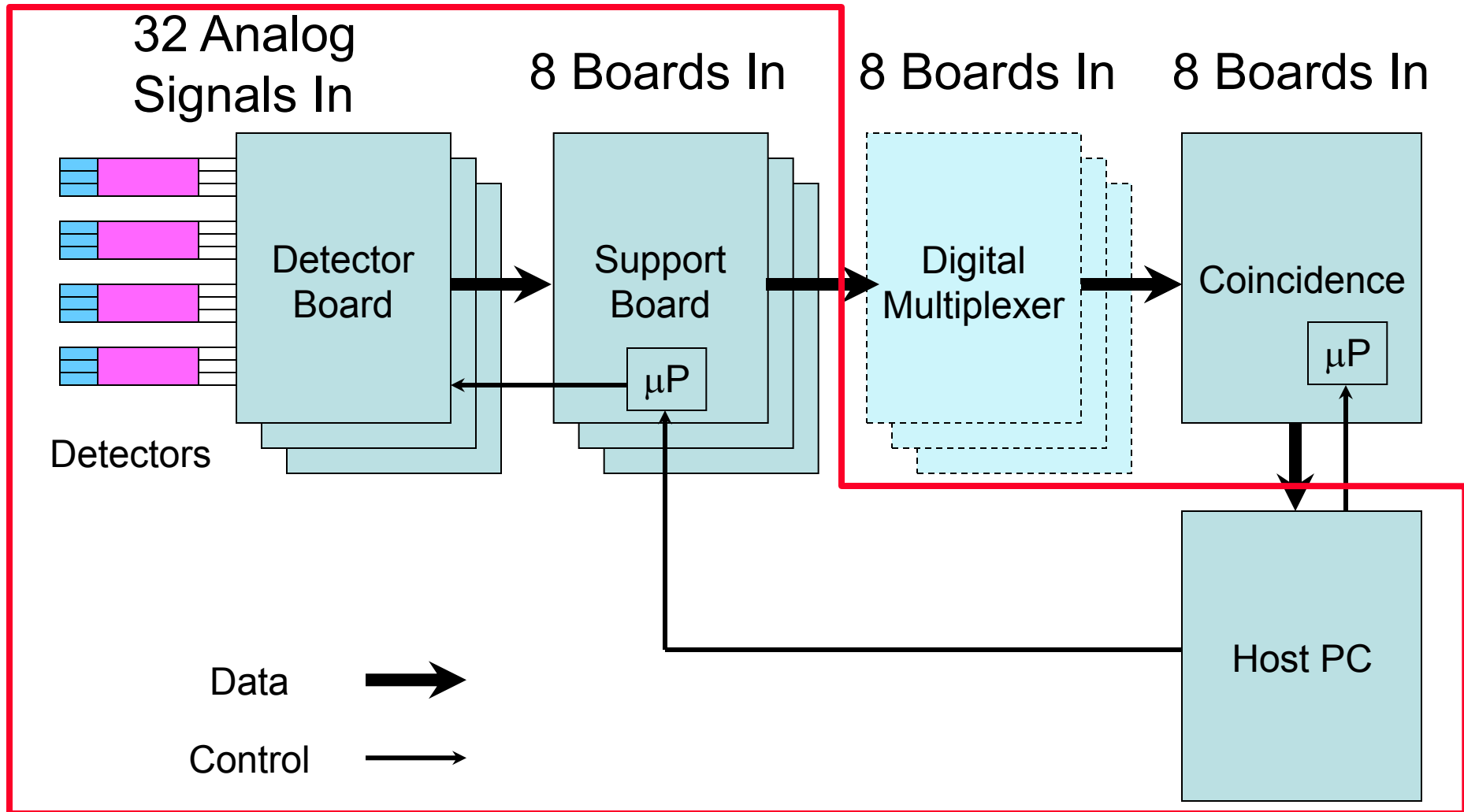
Extract Timing Signal
from Leading Edge

Extract “Energy” from
Area Under the Curve



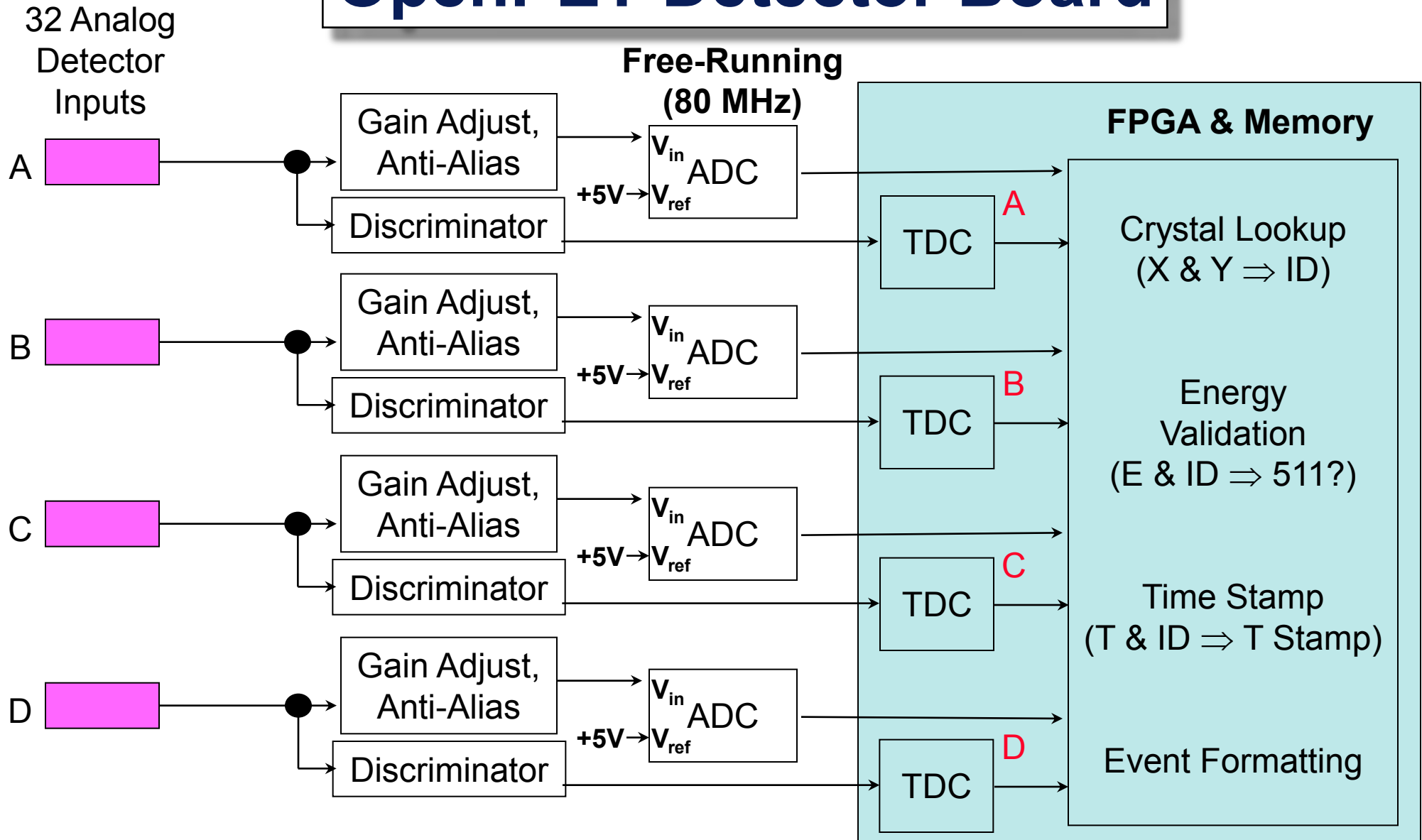
- ***Tremendous* Variation in How Outputs Are Combined**
⇒ **Digitize, Then Combine Outputs in Firmware**

OpenPET System Architecture



- Supports 512 Block Detectors (4096 With Multiplexers)
- SB + 8 DBs Makes Nice Test Stand (64 Block Detectors)

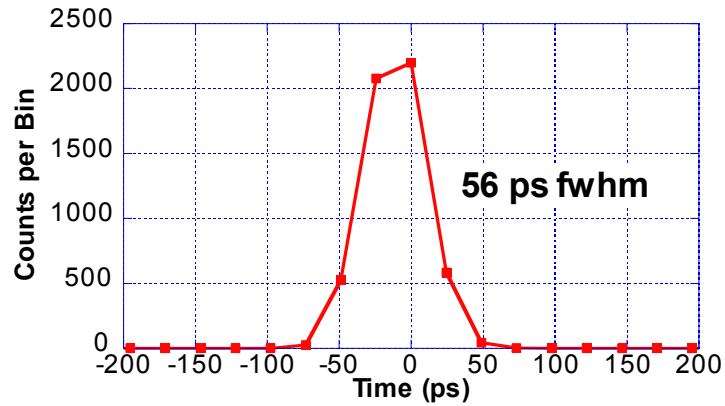
OpenPET Detector Board



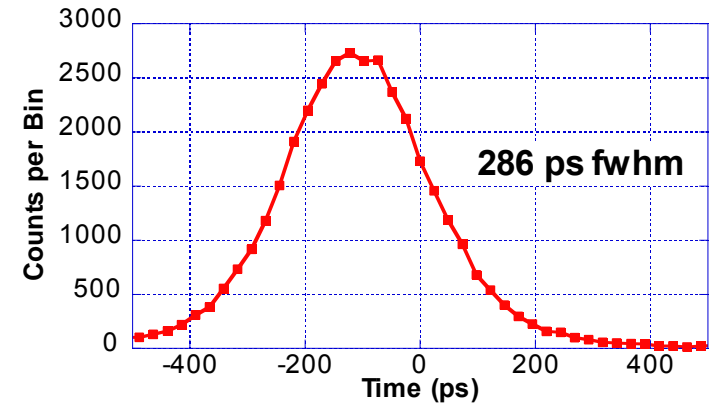
All Inputs Have Individual ADC, LE Discriminator, & TDC

Timing Resolution

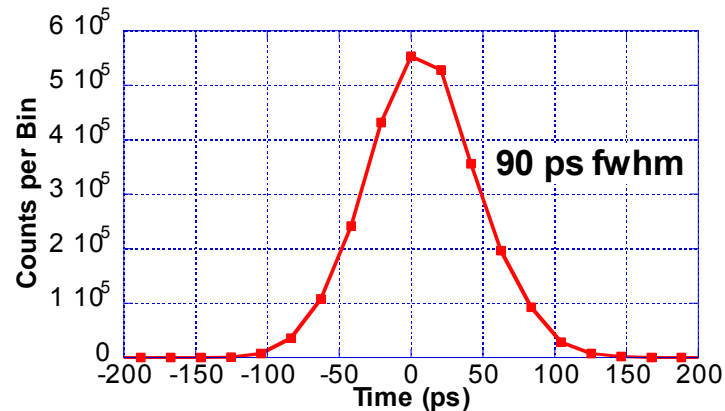
Test Pulse



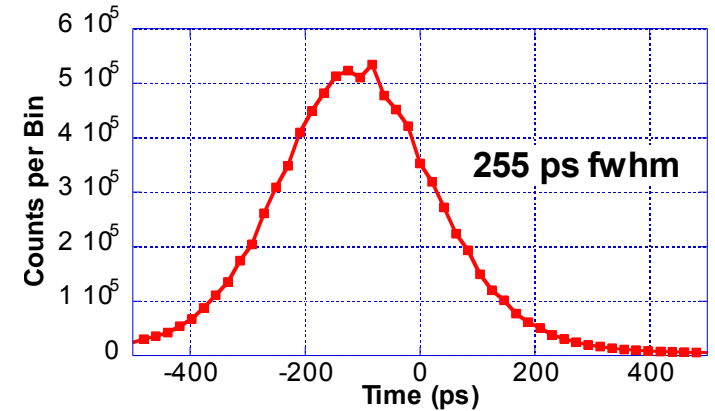
TOF Module Pair



**HPTDC
(CERN)**

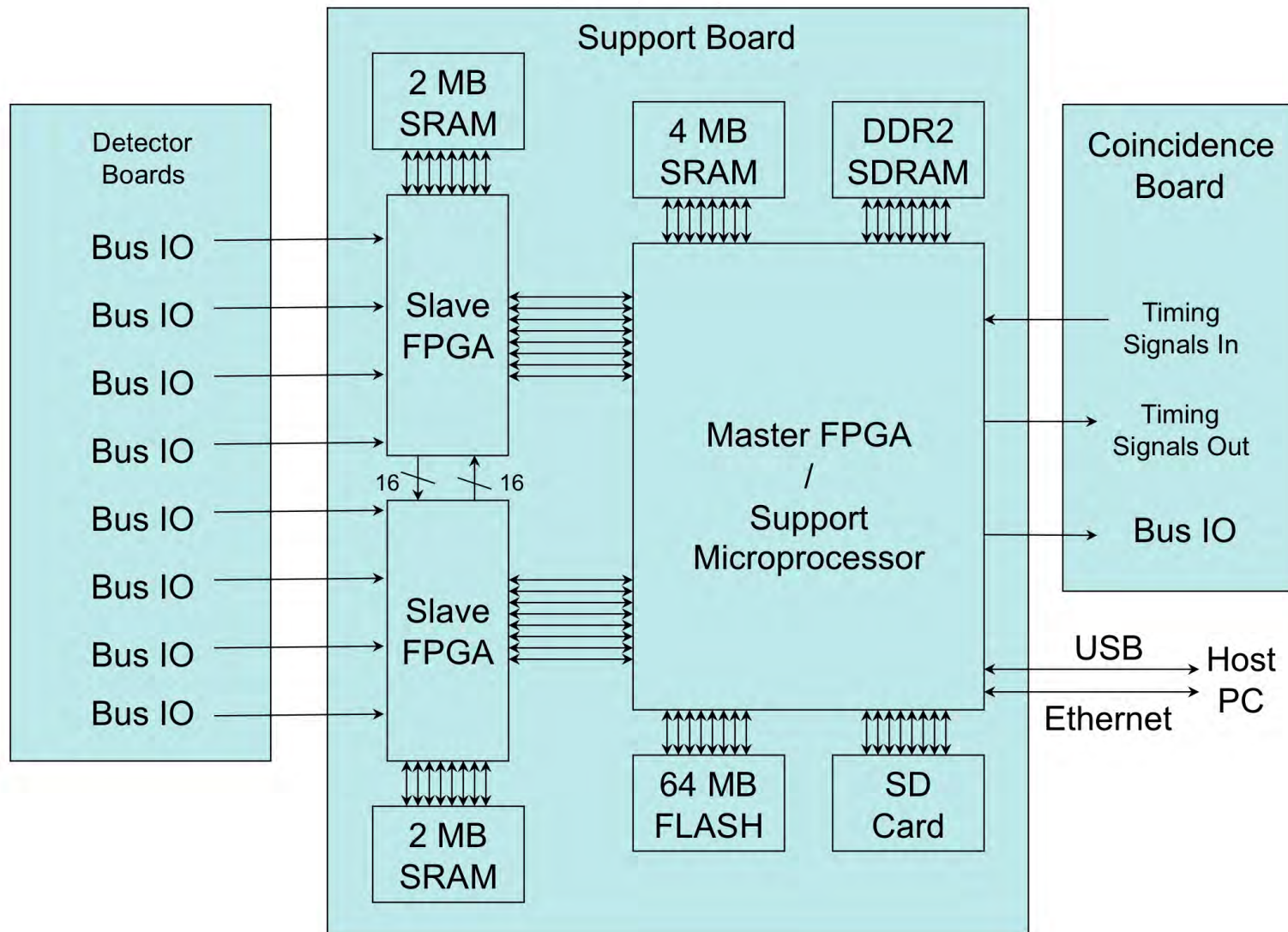


FPGA



- **32 Channel TDC in Cyclone II FPGA**
- **Performance Good Enough for Time-of-Flight PET**

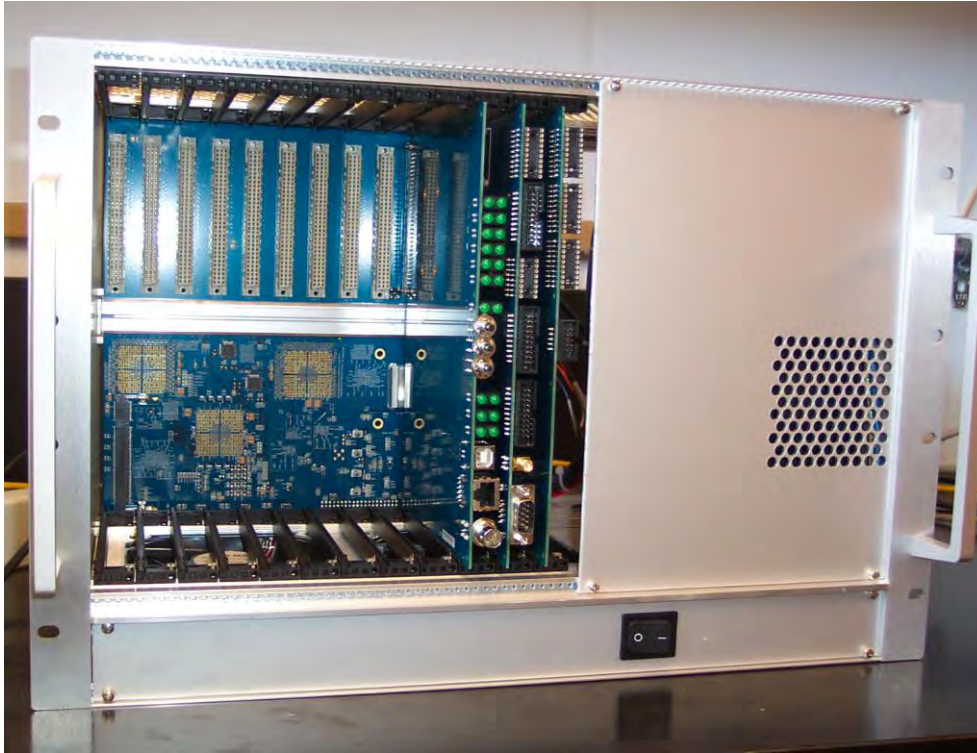
OpenPET Support Board



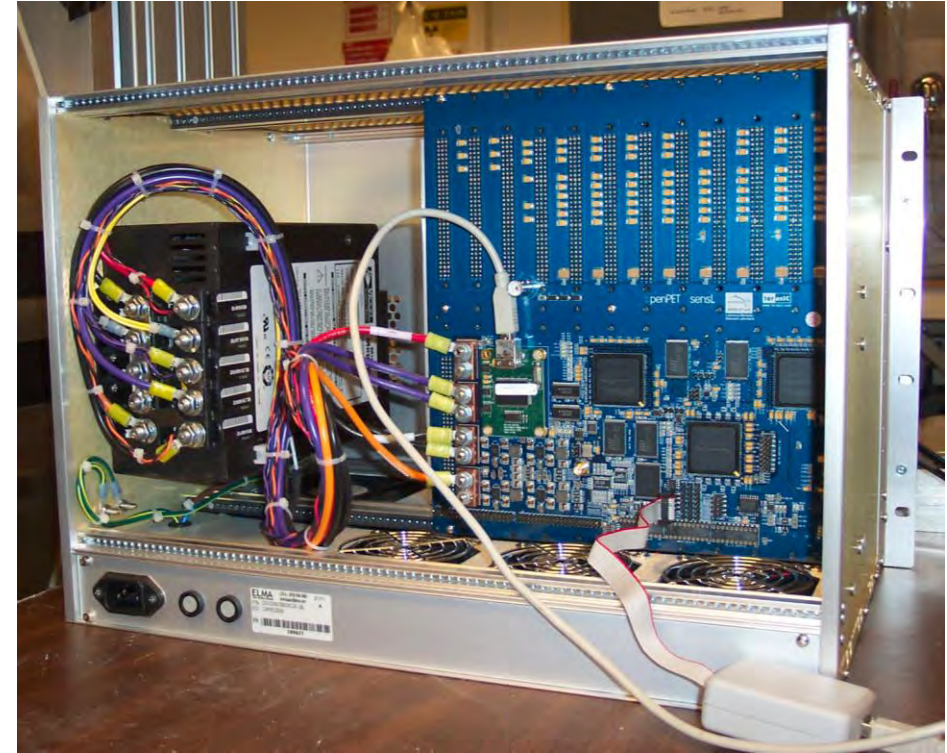
Resembles a PC Motherboard...

Support Board Designed, Built, & Tested

Front View



Back View



Slot 1–8: Detector Boards

Slot 9: Coincidence Board Interface

Slot 10: PC Interface (USB, Ethernet, SD Card, Detector Bias, 20 LEDs)

Slot 11: User Digital I/O (2 RS-232, 48 Digital I/O, External Clock In)

Slot 12: Debugging (JTAG, 4 Logic Analyzer Connectors, 30 LEDs)

VME Form Factor to Reduce Cost

openPET Vision

Open Source

- Hardware, Firmware, and Software
- Schematics, Gerbers, BOM,...

Active User Community

- Share Software and Expertise
- Module, Calibration, DAQ, Display,...

Hardware Readily Available

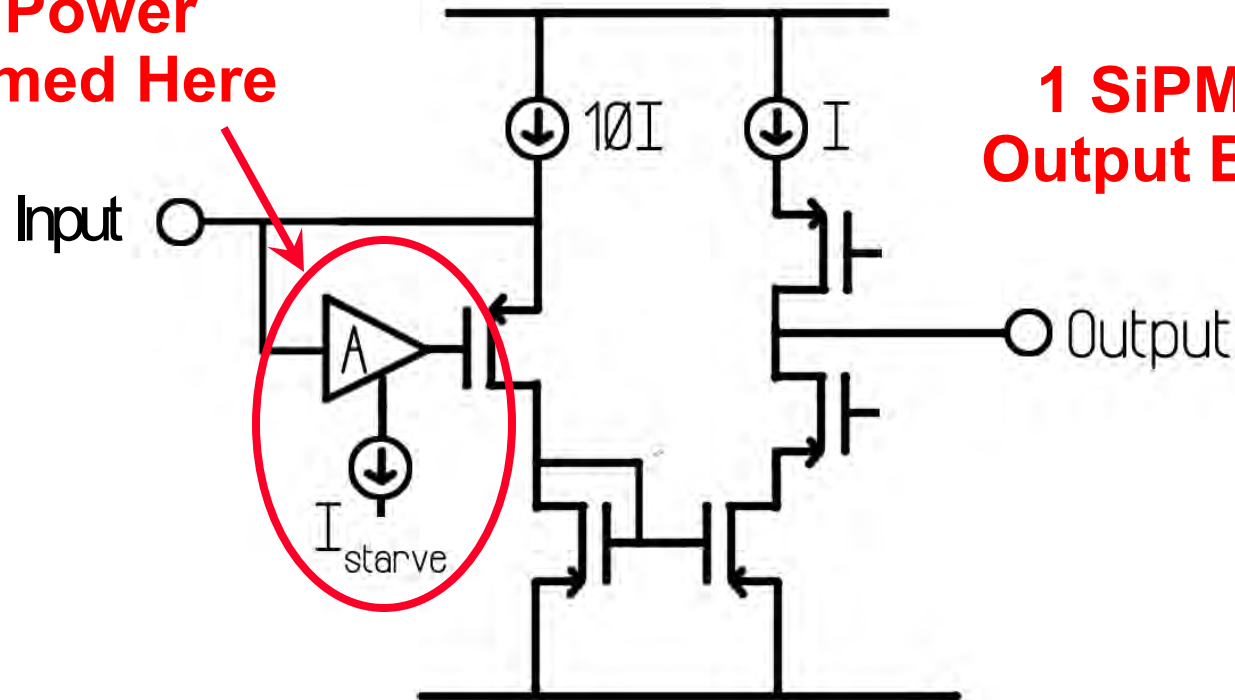
- Support Boards Available Now
- Detector Boards Available Spring 2012

<http://OpenPET.LBL.gov>



ASIC Achilles Heel: Power Consumption

~All Power Consumed Here



1 SiPM Pixel = 12 mW
Output Buffers = 120 mW

- Amplifier power proportional to pixel capacitance (& bandwidth)
 - Pixel capacitance proportional to area
- ➔ Power / area is constant ($75 \text{ mW} / \text{cm}^2 \rightarrow 500 \text{ W} / \text{PET camera}$)

How Can We Reduce Power / Area?

Conclusions

SiPM Readout ASIC Front-End Electronics

- **Current Division → 16x Lower Channel Count**
- **16 Channel Prototype Fabricated & Tested**
- **64 Channel ASIC Recently Received**
- **75 mW / cm²**

OpenPET Back-End Electronics

- **“Open Source” Electronics for Nuc. Med.**
- **Programmable – Extensive Use of FPGAs**
- **Support Boards Available Now**
- **Detector Boards Available Spring 2012**