A Spectroscopic Study of Prompt Gamma Emission for Online Range Verification in Proton Therapy

Laurent Kelleter Physics Institute III B, RWTH Aachen University IMPRS Munich mini-workshop 26/07/2016



Introduction to Ion Therapy and Prompt Gammas

Setup at Test Beam Time at HIT

Analysis of Prompt Gamma Spectra

Conclusion and Outlook



Introduction to Ion Therapy

- Radiation therapy is one important method to treat malignant tumors
- Advantages of ion therapy comparing to x-rays:
 - Biological effectiveness: Double-strand breaks (heavy ions only)
 - Physical: Dose distribution (all ions)



Dose distribution of different radiation typesLevin et al (2005): "Proton beam therapy". In: British Journal of Cancer.







Need for On-line Range Verification

- Steep slope after Bragg Peak makes ion therapy susceptible for range errors
- Today: In-beam PET after irradiation
- Future: On-line beam monitoring desired
- Approach: Prompt gammas emitted during ion therapy



Density effect on x-ray and carbon ion dose distribution HZDR, https://www.hzdr.de/db/Cms?pOid=11326&pNid=158



Prompt gammas emitted during ion therapy used for online beam monitoring http://medicalphysicsweb.org/cws/article/research/49909





Introduction to Prompt Gammas

- Prompt gammas are emitted by nuclear reactions
- Cross section of prompt gamma emission is proton-energy dependent
- Far goal: On-line range verification device for ion beams, e.g. Compton camera
- First phase: Study prompt gamma emission using High-Purity Ge detector



GEANT4 Simulation of 4.4 MeV prompt-gamma emission in PMMA (Sabine Feyen)







HPGe Detector with Active Compton-Shield





High-Purity Germanium Detector:

- Energy resolution better than 2 keV @ 1 MeV
- Surrounded by Active Compton-Shield (ACS) in order to reject Compton events





Setup during Test Beam at HIT 2015



- 1 Proton pencil beam (70 and 130 MeV)
- 2 Adjustable target thickness (wedges)
- 3 Thin target slice
- 4 HPGe detector to measure prompt gamma radiation from thin slice
- 5 Detector rotation system







Setup during Test Beam at HIT 2015



Proton pencil beam (70 and 130 MeV)
Adjustable target thickness (wedges)

- 4 HPGe detector to measure prompt gamma radiation from thin slice
- 5 Detector rotation system











PMMA target, 70 MeV beam energy, 120° observation angle

• Background measurement (blue): Measurement without slice in beam path







PMMA target, 70 MeV beam energy, 120° observation angle

• Background measurement (blue): Measurement without slice in beam path





Gamma Spectrum



- Background measurement (blue): Measurement without slice in beam path
- Gamma yield = Integral of prompt gamma peak





Depth Profile



- Vertical red line: Proton range in PMMA for 70 MeV beam energy
- Steep slope behind maximum gamma yield in both cases!





Overview of Experimental Data Test Beam HIT 2015







Dependence on Chemical Composition



70 MeV beam energy, 90° detection angle





Dependence on Beam Energy



PMMA, 90° detection angle

- Reduced integral because of elimination of protons from the beam
- Broadening of the profile because of stochastic energy loss





Dependence on Detection Angle $\boldsymbol{\theta}$



PMMA, 70 MeV beam energy

- Single-slit- and Compton camera observe multiple angles at once!
- $\theta \neq 90^{\circ} \Rightarrow$ complex reconstrution algorithms and a decrease in spatial resolution





Conclusion and Outlook

- Achieved:
 - Successful measurement of the depth profiles for ${}^{12}C_{4.44 \rightarrow g.s.}$ and ${}^{16}O_{6.13 \rightarrow g.s.}$ -lines
 - Steep slope behind maximum gamma yield seen for all studied reactions and measurement conditions
 - Strong influence of phantom composition on ${}^{12}C_{4.44 \rightarrow g.s.}$ peak shape
 - Depth profile characteristics at increasing beam energy studied
 - Influence of detection angle on depth profile studied
- Outlook / ongoing:
 - Publish paper about results (currently in peer review by Phys. Med. Biol.)
 - Upgrade setup and go for next beam time
 - Derive conclusions and start with setup of a gamma/Compton camera



Thank you for your attention!



The project "Investigation of gamma emission in experimental modeling of hadron therapy" is carried out within the POMOST programme of the Foundation for Polish Science, co-financed from the European Union under the European Regional Development Fund.

Backup

Heidelberger Ionenstrahl-Therapiezentrum (HIT)



Heidelberger lonenstrahl-Therapiezentrum. https://www.klinikum.uni-heidelberg.de/Accelerator-facility.117968.0.html?&L=1





Target Material

Material	Chemical composition	Density / g cm ⁻³	Slice thickness / mm
PMMA	$(C_5O_2H_8)_n$	1.19	2
POM	(CH ₂ O) _n	1.43	1
Graphite	Ċ	1.74	1



POM target wedges

POM thin target slice







Normalization and Calibration of Gamma Spectra

- Normalization: Use Beam Current Monitors and HIT calibration files
 - \rightarrow Normalization to number of protons in beam
- Calibration:
 - Pre-calibration using 4 caracteristic peaks in a single run (Anna Chrobak, Katowice)
 - Identification of reaction peaks in spectrum (mainly Daniel Böckenhoff Master's thesis)
 - Calibration performed for each run separately using 8 characteristic peaks
 - \rightarrow Systematical shifts of 6.1 MeV peak position below 5 keV over whole beam time







Background Parametrization

- Background is measured at different target thicknesses \Rightarrow parametrization needed
- Automatized fit of error function implemented

• $f(x) = \frac{2}{\sqrt{\pi}} \int_0^x e^{-\tau^2} d\tau$



Background for 4.4 MeV peak of Graphite, 70 MeV beam energy, 120 $^\circ$ observation angle







Investigation on angular effects



Angular dependence of

- peak integral (angular distribution)
- peak shape (coherent Doppler effect: 4.4-gamma emitted by carbon atom in-flight after collision with proton)



Physics

Institute III B



Angular Distribution



PMMA, 70 MeV beam energy

 \Rightarrow Backward detection angles give higher gamma output!



Performance of Active Compton-Shield

